

HORIZONTAL ALVEOLAR BONE AUGMENTATION USING GUIDED BONE REGENERATION FOLLOWING ALVEOLAR BONE DECORTICATION OR DEMINERALIZATION (CLINICAL AND HISTOLOGICAL STUDY)

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ABSTRACT

Background: Bone volume affects the long term success of an implant. Augmentation of the existing edentulous alveolar bone is often necessary to obtain excellent functional and esthetic restorations of the implants. The reconstruction of alveolar ridges for implant placement is still a challenging procedure, especially in the case of extensive vertical and horizontal atrophy. Here, we aimed to evaluate the effect of EDTA bone demineralization on bone graft consolidation to the native bone in comparison to alveolar bone decortication.

Methods: A total of 14 subjects were divided into two groups (n = 14) . In the test group I (n = 7), alveolar cortical bone in the area of regeneration was demineralized by 24% EDTA. While, decortication was performed in group II (n = 7). Subsequently, defects in both groups were augmented by guided bone regeneration using resorbable membrane and bovine bone. After a healing period of 6 months, trephine cores were harvested for histological and histomorphometric analysis of the grafted areas and the buccolingual width dimension was evaluated radiographically

Results: Histomorphometrical analysis demonstrated that the amount of newly formed bone in the test group (3.63 ± 1.35 %) was greater than that in group II (2.52 ± 0.78 %), and the difference was statistically significant ($P = 0.029$)

Conclusions: Bone demineralization results in more width gain than mechanically decorticating the alveolar bone.

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INTRODUCTION

After tooth extraction, a process of remodeling of alveolar bone occurs which result in horizontal and vertical bone resorption (*Van der Weijden et al., 2009; Liu and Kerns, 2014*). *Carlsson* and his colleagues studied changes of the mandible after tooth extraction. The percentage of bone resorption was estimated as 21 % after 3 months, 36% after double this period, and 44% after 1 year (*Carlsson and Persson, 1967*). The most dimensional tissue changes (about 50%) happened at the extraction site during the first year after tooth extraction (*Schropp et al., 2003*) Studies concluded that the amount of horizontal bone resorption is higher than the amount of vertical bone resorption clinically as well as radiographically (*Van der Weijden et al., 2009*).

Endo-osseous dental implants have been a good solution to restore missing teeth. The bone volume affects the long term success of an implant. In case of bone volume inadequacy, additional techniques may be implemented to reach acceptable outcomes. Accordingly, local bone augmentation, accompanied by guided bone regeneration, has been brought into consideration (*Lekholm et al. 1999*).

Both the morphology of the bone defect and the ridge contour dictate the best treatment protocol and the selection of materials (*Benic and Hämmerle, 2014*). It had been determined that the least dimensions for inserting cylindrical implants are 5-8 mm in height and 6 mm in width. Alveolar bone 1 mm thick should encircle the implant after insertion. Therefore, widening of the alveolar ridge before implant insertion is mandatory in cases of ridge width of 4 mm or less. Alveolar ridge augmentation is highly recommended, if implant stability or appropriate positioning cannot be achieved. (*Bahat 1994; Miyamoto et al., 2012*).

Procedures that use barrier membranes to direct the growth of new bone toward sites of bone defects is called Guided bone regeneration (GBR). This is done to restore function and esthetics. (*Dahlin et*

al., 1988; Miloro et al., 2004). To ensure successful GBR, four principles need to be met ,these are, wound closure, blood supply maintenance of space, and stability of the initially formed blood clot (**PASS principle**) (*Wang and Boyapati, 2006*).

Different materials have been used in studies in terms of GBR. Barrier membranes can be classified into three generations. First generation membranes are non-absorbable membranes, that were used for periodontal regeneration. These include cellulose acetate (Millipore), expanded polytetrafluoroethylene (e-PTFE), titanium reinforced ePTFE, high density- PTFE. Second generation membranes are absorbable membranes, which could be natural such as collagen or synthetic which are made from polyester such as polyglycolic acid (PGA), poly-lactic acid (PLA) and their copolymers. Third generation membranes act as barriers and as delivery vehicles for local agents such as antibiotics and growth factors (*Scantlebuty, 1993; Hardwick et al., 1995; Saad et al., 2012; Sam and Pillai, 2014*)

Non-resorbable membranes are not biodegradable, that is, they require another surgical intervention to be removed. Moreover, their exposure may lead to total failure of the regeneration process (*Rocchietta et al., 2008*).

Resorbable membranes do not require a second procedure to remove the membrane. It requires less surgical time with less potential postsurgical morbidity (*Tolstunov et al., 2019*). However, their limitations include, uncontrolled duration of barrier function and the need of a membrane supporting material to minimize its failure. (*Schwarz et al. 2006; Becker et al. 2009*).

Pericardium membrane has been utilized as a part of cardiac repair. The xenogenic pericardium is derived from bovine sources. It includes collagen strands, and has elastic properties enabling adjustment to complex anatomy (*Nair 2018*).

Bone graft materials function as scaffolds that maintain space for osteogenic cells, and the host response to these scaffolds is accordingly one of the success factors in GBR (*Hockers et al., 1999; Esposito et al. 2009*).

Bone fillers could be autogenous bone chips, allograft (same species), xenograft (another species), or alloplast (synthetic). They are commonly used in the GBR process. They promote bone ingrowth and healing through osteoconduction, by offering mechanical support of the membrane and stabilizing the blood clot (*Jensen et al., 2006*).

The gold standard material is the autogenous bone as it is the only type of graft that has osteoconductive, osteoinductive and osteogenic potential (*Brunsvold and Mellonig, 1993; Pandit and Pandit 2016*). The main drawbacks of autogenous bone grafts are the limited bone volume availability that can be obtained and the morbidity of the harvesting site (*Dragoo and Sullivan, 1973; Jensen et al., 2016*).

Allografts are fresh, frozen-fresh, freeze-dried grafts that are harvested from two dissimilar members of the same species. The main problem with fresh and frozen allografts was the immunologic potential that could occur when used. This could lead to complications such as, graft infections, a nonunion or, delayed union at the graft host interface (*Lord et al. 1988; Aro and Aho 1993; Gazdag et al., 1995; Kumar et al., 2013*).

Xenografts are grafts that are obtained from another species which could be bovine, porcine, equine or coralline. Chemical and physical properties of xenografts were found to be similar to that of human bone, when used they provided osteoconductive properties (*Traini et al., 2007; Wong and Griffiths, 2014*). Alloplasts are synthetic inorganic graft substitutes which have osteoconductive properties. They can be made from ceramic based materials such as calcium phosphates {hydroxyapatite (HA), tricalcium phosphate} and

bioactive glass or they can be made from polymer based material which can be either natural or synthetic (*Kumar et al., 2013*).

For attaining GBR, angiogenesis and adequate blood supply are of prime importance as they follow a sequence of events. In 1994, *Schmid et al.*, concluded that new bone regeneration is mainly dependent on the development of new blood vessels that stimulate and nurture the surgical site. 24 hours after a GBR procedure, a blood clot is formed then it is resorbed by neutrophils and macrophages and hence is replaced by granulation tissue containing numerous blood vessels that transport cells and nutrients involved in bone matrix formation. Osteoid is unmineralized bone matrix and is referred to as woven bone upon mineralization. Woven bone acts as a scaffold. (*Schmid et al., 1994; Hämmerle et al., 1995 ; Schmid et al., 1997*). Regeneration of new bone is established after 4 weeks from initiating GBR (*Hämmerle et al., 1995; Hämmerle et al., 1996; Schmid et al., 1997; Glowacki, 1998; Lu et al., 2007*).

Bone decortication is done by drilling holes through the cortical bone into the spongy bone or by complete removal of the cortical bone. Bone decortication has been used as a part of GBR and stated in several cases to enhance the ridge thickness and height prior to implant placement (*Buser et al., 1990; Buser et al., 1993; Buser et al., 1995; Greenstein et al., 2009*).

Many trials stated that bone decortication resulted in increased apposition of lamellar bone in the grafted site. The new bone formation was related to regional acceleratory phenomena after traumatizing the alveolar bone mechanically by making bone perforations. Bone decortication in GBR allows the release of bone and blood forming cells from the bone marrow space, resulting in the synthesis of the new bone matrix (*Frost, 1983; Buser et al., 1990; Greenstein et al., 2009; Saghir et al., 2016*).

Localized osteoporosis is a part of the healing process, that can accelerate hard and soft tissue healing two to ten times. The mechanical interlocking of a bone graft and a recipient site can be increased by perforating the bony cortex and may also improve its stability by firm bonding to the newly formed bone. Bone decortication improved mineralized bone and newly regenerated augmented tissue during guided bone regeneration (*Alberius et al., 1996; Amit et al., 2012; Acar and Yolcu, 2018*).

On the other hand, decortication has some disadvantages such as long operating time, extra blood loss, increased postoperative pain, and some bone loss in case the procedure fails. *Maestre-ferrin et al.*, observed that the union of onlay bone graft to the recipient bed does not have adequate strength to maintain adequate integrity when preparing the surgical sites and or implant placement due to shear forces produced during those procedures and may lead to detachment of the bone graft (*Greenstein et al., 2009; Maestre Ferrín et al., 2009*).

Therefore, authors used other ways not to mechanically treat bone by decortication but chemically by means of acid demineralization of alveolar bone cortex surface to enhance bone formation and integration (*Greenstein et al., 2009*)

The extracellular matrix of bone contains a reservoir of growth factors. Following trauma, these proteins, such as platelet derived proteins, bone morphogenetic proteins, insulin like growth factors and transforming growth factor- β (TGF- β), target cells in the injury site. (*Hauschka et al., 1986; Frolík, Ellis, and Williams 1988; Taipale And Keski-Oja, 1997; Schonherr and Hausser, 2000; Ramirez and Rifkin, 2003*).

Citric acid, (EDTA), and calcium hydroxide have the ability to dissolve TGF- β 1 from dentine. They act by mineral demineralization or calcium chelation. TGF- β 1 released from dentine after calcium hydroxide treatment differs in level than that released after the use of EDTA (*Zhao et al.,*

2000; Graham et al., 2006; De-Deus et al., 2008).

In 1965, *Urist et al.* was the pilot to introduce the principle of intentional bone demineralization, when HCl was used to decalcify bone grafts implanted in animals subcutaneously. Bone demineralization could have osteoinductive potential where demineralization is done using diluted acid which removed inorganic component of bone (*Urist and McLean, 1965*).

Urist et al in 1970, tested the induction of new bone formation after a demineralized bone or dentin matrix was implanted in rabbit muscles. Results had showed ectopic new bone formation intramuscular after 4 to 6 weeks from implantation. In a sequence of studies, this induction was found to be a result of the released bone morphogenic proteins to the surrounding environment as a result of the bone demineralization process (*Urist et al., 1970; Urist, 1973*).

The physiologic mechanism of bone remodeling involves demineralization by acid production from osteoclasts. These acids attack minerals and release enzymes on the bone surface, that hydrolyze the organic matrix (*Roodman, 1999; Hadjidakis and Androulakis, 2006*). Preosteoblasts differentiate on a rough surface and deposit new bone. It was found that demineralization with tetracycline resulted in surface roughness comparable to that produced by osteoclasts acting on dentin. (*Schwartz et al., 2000*).

In 2015, *Rezende et al.*, stated that demineralization by citric acid resulted in surface roughness equivalent to that produced by osteoclasts during bone resorption.

Osteoinductive property was stated to be due to the exposure of certain proteins found in the bone matrix which stimulated the surrounding mesenchymal cells to differentiate to osteoblasts and produce new bone (*Bauer and Muschler, 2000*). Superficial bone demineralization has been revealed

to be a promising adjunctive during regenerative procedures. In addition to the favorable biological effects presented above, some relevant advantages of bone demineralization can be cited as: the low cost of the acid solutions, the ease of its clinical use, as there are no need for perforations or decortication of the bone bed, the resorption of the bone grafts is minimized as the demineralization mimics osteoclasts function, there is an anticipation of the remodeling events and consequently, a reduced healing time (*Salmeron and Rezende, 2017*)

EDTA (Ethylene di-amine tetra-acetic acid) gel preparation was studied as a root surface conditioning material because of its neutral PH that would not damage the organic component of the root, accompanying surgery following conventional flap in PDL intraosseous defects, the results showed bone gain of about 1mm to 1.5mm. Scanning electron microscope study of root dentine revealed dentinal tubule opening free from smear layer and collagen fiber exposure in the intertubular dentin (*Blomlöf et al., 1997; Mayfield et al., 1998*).

Increased surface exposure after treatment of bone surfaces with either EDTA or calcium hydroxide resulted in the release of active growth factors, having more osteogenic effect on bone marrow stromal cells. EDTA and citric acid have shown similar patterns of TGF- β 1 surface dissolution. (*Smith et al., 2011*).

Owing to the lack of necrotizing effect of EDTA etching, it is more beneficial to periodontal and bone healing because of its ability to selectively expose collagen fibers in dentin and bone, which in turn produces a matrix to retain implants of biologically active substances and provides a biocompatible surface for periodontal membrane cell colonization (*Blomlöf, 1996; de Vasconcellos et al., 2006*).

So, the current study aimed to evaluate the effect of demineralization of alveolar bone in comparison to bone decortications prior to bone graft application in cases that needs horizontal ridge augmentation.

MATERIALS AND METHODS

The study consisted of 14 subjects (age range: 25-55 years) attending the outpatient clinic of Oral Medicine and Periodontology department, faculty of Dentistry, Ain Shams University, Cairo, Egypt. Those who agreed to participate voluntarily have written informed consent and ethical clearance, FDASU-Rec1M011613, was obtained from the Institution's Ethical Committee. Inclusion criteria include subjects: 1- free from any systemic disease as evidenced by health questionnaire using modified Cornell Medical Index (*Abramson, 1966*). 2-Single lower posterior edentulous area, for more than 6 months since the time of extraction with remaining 5 mm or less in horizontal dimension. 3- Sufficient zone of attached gingiva (*Bouri et al., 2008*). Patients with previous medical history and patients who had any systemic or local factors that would inhibit a normal wound healing process were excluded.

They were randomly assigned into two groups: test patients (n = 7) received EDTA etching of the recipient bed; Group II patients (n = 7) had perforation of the recipient bed prior to GBR. using computer generated random tables (IBM SPSS statistics for windows, version 22.0. Armonk, NY: IBM comp).

Each subject underwent a full mouth scaling and debridement. Presurgical baseline tomography CBCT was taken to determine the severity of ridge resorption at the osteotomy site. Measurements were taken 1mm subcrestal, at the middle of the mesiodistal, buccolingual edentulous area.

After administration of local anesthesia, intrasulcular, crestal and 2 vertical releasing incisions were done to elevate a full thickness periosteal flap and expose the recipient bone. The intrasulcular incision was extended two teeth mesial or distal to the defect. The buccal flap was extended beyond the mucogingival junction and at least 5 mm

beyond the bone defect (*Urban et al., 2013*). For group I, after isolation of the field, the bone surface was etched by application of EDTA*, 24% (PH 6.7) for 1 minute to the bone surface (*Blomlöf et al., 1997*). (**Fig.1**)

For group II, decortication of bone surface was done by size 2 round bur** to induce bleeding under copious water irrigation. (**Fig.2**)

Subsequently, Bovine pericardium membrane (Tutopatch, tutogen medical GmbH, Germany) was inserted and fixed with fixation pins (Titan, Botiss, Germany) at the apical part of the defect. Particles (particle size 0.5–1 mm) of deproteinized bovine bone (Cerabone, Botiss, Germany) were placed in the defect area and covered by the membrane. A tension-free primary closure was achieved and the flap was sutured with non-resorbable suture material (Polypropylene blue, Assut medical, Switzerland). (**Fig.1: I&II**)

The patients were instructed to have Augmentin 1gm twice for 7 days, (ibuprofen 600 mg) for 3 days and to rinse with 0.12% chlorhexidine digluconate oral rinse 3 times daily for 2 weeks. Postoperative examination and suture removal were performed after 14 days.

6 months later, (mean months), patients were clinically assessed for any local problem that might interfere the surgical intervention. Before implant placement, a CBCT was taken for both groups to assess the width of alveolar ridge and for implant planning.

Bone core samples (2 mm in diameter and 5 mm in length) were obtained from within the boundaries of the augmented site using a trephine drill, under copious irrigation, without compromising implant placement. (**Fig.1: III&IV**)

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Dental implants (Neobiotech), were placed according to standard protocols in a prosthetically ideal position and the flap repositioned and sutured. All biopsy specimens were placed in 10% neutral

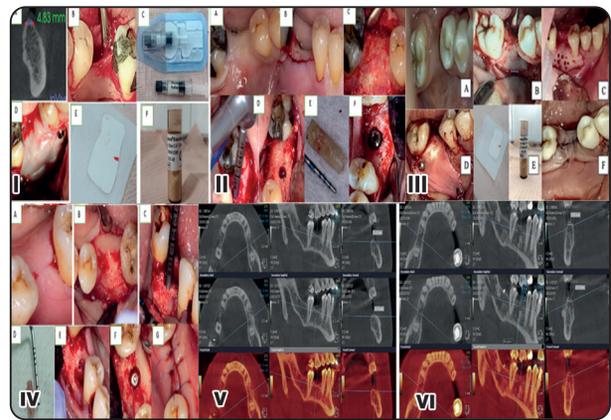


Fig (1: I): EDTA group. **a** Coronal slice of the site of implant that needs GBR. **b** Mucoperiosteal flap reflection. **c** Showing the EDTA 24% gel (Prefgel). **d** Showing Pericardium membrane fixed with tacks in place supported by the underlying bone graft material. **e** The Tutopatch membrane & the demineralized bovine bone mineral (DBBM) (Cerabone, Botiss, Germany).

Fig (1: II): Decortication group. **a** Site of implant that needs GBR. **b** Mucoperiosteal flap reflection. **c** decortication of the buccal surface of cortical bone. **d** Pericardium membrane fixed with tacks in place supported by the underlying bone graft material. **e** The Tutopatch membrane & the demineralized bovine bone mineral (DBBM) (Cerabone, Botiss, Germany). **f** Immediate postoperative suturing of the flap using 4-0 propylene blue suture

Fig (1: III): EDTA group Re-entry. **a** the augmented site of missing lower left first molar. **b** Mid-crestal incision of the augmented site. **c** Showing the alveolar ridge width gain 6 months after GBR procedure. **d** Showing the site of core biopsy intake using trephine bur drill. **e** Showing 7 mm length core biopsy **f** Showing the augmented site received a dental implant.

Fig (1: IV): Decortication group Re-entry. **a** Showing the augmented site of missing lower left first molar. **b** Showing the alveolar ridge width gain 6 months after GBR procedure. **c** Showing the site of core biopsy intake using trephine bur drill. **d** Showing core biopsy. **e** Showing the augmented site received a dental implant. **f** Postoperative suturing.

Fig (1: V&IV): **V** : **a** showing the superimposition method between T1&T2 for group I. **IV** showing the superimposition method between T1&T2 for group II

buffered formalin for 5 days to fix the dissected block sections.

CBCT taken at reentry were assessed by fusion method for buccolingual width dimensions after mean of 6 months.

For histological studies, the specimens were cleared with xylene and embedded in paraffin wax. 4 microns thick Sections were cut longitudinally using a Jung K microtome (Leica microtome type sm2500s; Leica, Wetzlar, Germany). The prepared slices were stained with haematoxylin and eosin (H&E) and observed by a light (Carl Zeiss, Oberkochen, Germany). (This was done in the Oral Histology laboratory, Oral Biology Department, Faculty of Dentistry Ain Shams University.

All clinical and biochemical data were tabulated and statistically analyzed.

Statistical analysis:

The averages and ranges for the percentage of newly formed bone, residual graft particles were calculated. Numerical data were presented as mean and standard deviation (SD) values. They were explored for normality by checking the data distribution, and using Shapiro-Wilk test. Data showed parametric distribution so they were analyzed using paired t-test. R statistical analysis software version 4.1.1 for Windows was used to obtain the statistical results.

RESULTS

All surgical sites healed without complications. No flap dehiscence and no exposure of membranes were noted. Good primary stability of all implants and after 4 months of healing were restored. No residual parts of the collagen membrane could be detected at re-entry surgery and the regenerated tissue appeared as mineralized bone tissue and enough to place implants without grafting.

Histological Assessment:

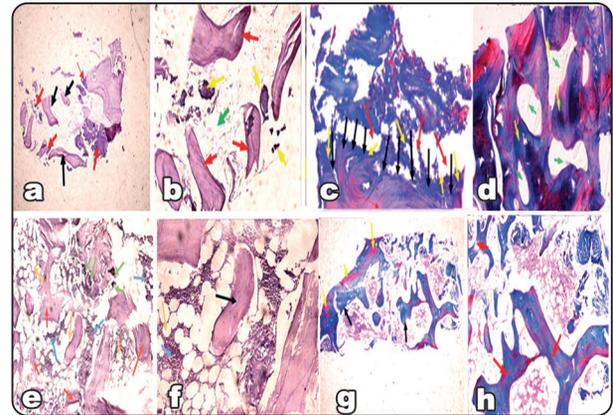


Figure (2)

Group I (EDTA): as shown in Figure (2: A, B,C,D)

Fig. (2: A&B) Photomicrograph of bone core biopsy taken after 6 months of horizontal augmentation. The newly formed bone trabeculae shown by red arrow surrounded by fat cells shown by green arrow and residual bone graft particles shown by the yellow arrows after 6 month **A:** (H&E stain org.mag.X100). **B:** (H&E stain org.mag.X400).

Fig. (2: C&D): Photomicrograph showing integration of the new collagen shown by yellow arrow on the surface of the native cortical lamellated bone as shown by the red arrow, the blue arrow represents the spaces of DBBM particles after decalcification. Black arrows represent the interface between native bone and bone graft. **C:**(Masson's Trichrome stain org.mag.X200). **D:** (X400). **Group II (Decortication):**as shown in (E, F,G,H).

Fig. (2: E&F): A photomicrograph showing islands of new bone shown by red arrow surrounded by inflammatory cells and fat cells. The blue arrow shows areas of inflammatory cells and the orange arrow shows areas of fat cells surrounding islands of new bone. Residual graft particles shown by green arrow. The black arrow showing an island of new bone surrounded by inflammatory cells as shown by the orange arrow and fat cells as shown by the blue arrow. **E:** (H&E stain org. mag.X200). **F:** (H&E stain org.mag.X400)

Fig. (2: G&H): Photomicrograph showing a biopsy stained by Masson's Trichrome stain. Black arrow shows areas of new collagen formation. Yellow arrow represents the native bone. Areas of new collagen formation shown by red arrow. **G:** (Masson's Trichrome stain org.mag. X100). **H:** (X400).

Histomorphometric analysis

The histomorphometric analysis was done by processing the images from the microscope with a camera (Olympus BX50; Olympus Optical Co., Tokyo, Japan) and a frame grabber. The images from each area of the biopsy core were obtained and analyzed using image analysis software (Image j) to calculate the percentages of residual graft particles (RG), area percentage of newly formed bone (NB), in each specimen.

- Group (I) (3.63 ± 1.35) had a significantly higher value of area percentage of new bone formation than group (II) (2.52 ± 0.78) ($p=0.029$).

TABLE (1): Mean, Standard deviation (SD) values of area percentage of new bone formation (%) for different groups

Area percentage of new bone formation (%) (mean±SD)		p-value
Group (I)	Group (II)	
3.63±1.35	2.52±0.78	0.029*

*; significant ($p \leq 0.05$) ns; non-significant ($p > 0.05$)

- Group (II) (0.63 ± 0.39) had a higher value of residual bone graft particles than group (I) (0.25 ± 0.03) yet the difference was not statistically significant ($p=0.186$).

TABLE (2): Mean, Standard deviation (SD) values of residual bone graft particles (%) for different groups

Residual bone graft particles (%) (mean±SD)		p-value
Group (I)	Group (II)	
0.25±0.03	0.63±0.39	0.186ns

*; significant ($p \leq 0.05$) ns; non-significant ($p > 0.05$)

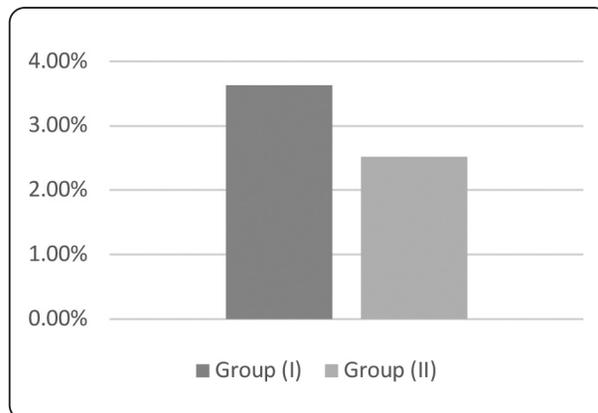


Fig. (3): Bar chart showing average area percentage of new bone formation (%) for different groups

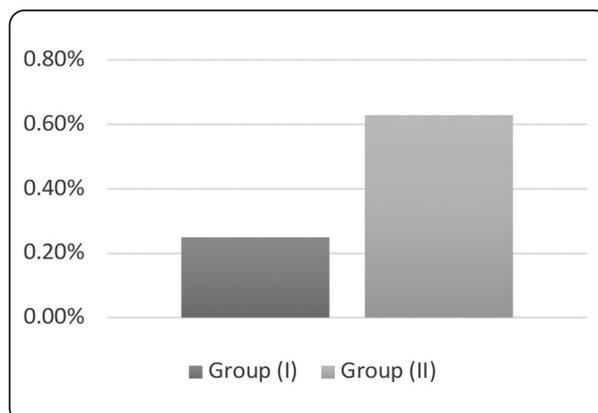


Fig (4): Bar chart showing average residual bone graft particles (%) for different groups

Radiographic Assessment

1- Intergroup comparisons:

Baseline:

Group (I) (4.81 ± 0.68) had a higher value than group (II) (4.40 ± 0.59) yet the difference was not statistically significant ($p=0.178$).

6 months:

Group (I) (8.17 ± 0.99) had a significantly higher value than group (II) (6.37 ± 0.77) ($p=0.001$).

Difference:

Group (I) (3.37 ± 0.61) had a significantly higher value than group (II) (1.97 ± 0.27) ($p < 0.001$).

2- Intragroup comparisons

Group (I)

Value measured at 6 months (8.17±0.99) was significantly higher than value measured at baseline (4.81±0.68) (p<0.001).

Group (II)

Value measured at 6 months (6.37±0.77) was significantly higher than value measured at baseline (4.40±0.59) (p<0.001).

TABLE (3) Mean, Standard deviation (SD) values of alveolar bone width (mm) for different groups

Interval	Alveolar bone width (mm) (mean±SD)		p-value
	Group (I)	Group (II)	
Baseline	4.81±0.68	4.40±0.59	0.178ns
6 months	8.17±0.99	6.37±0.77	0.001*
p-value	<0.001*	<0.001*	
Difference	3.37±0.61	1.97±0.27	<0.001*

*; Significant (p ≤ 0.05) ns; non-significant (p>0.05)

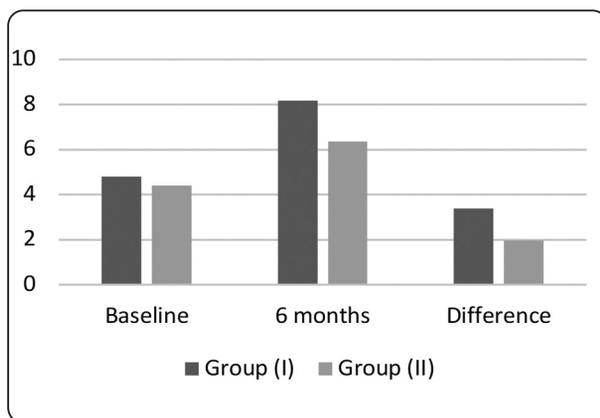


Fig (5): Bar chart showing average alveolar bone width in different groups

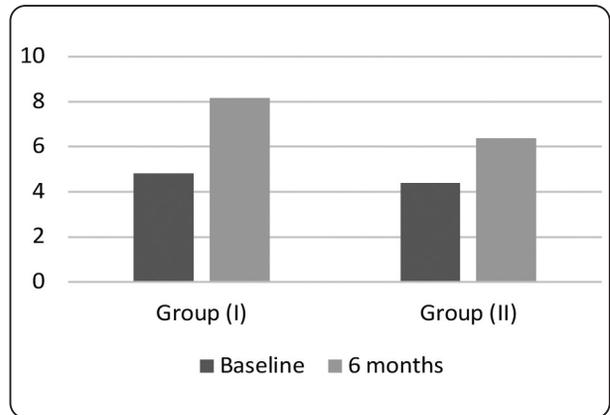


Fig (6): Bar chart showing average bone width change

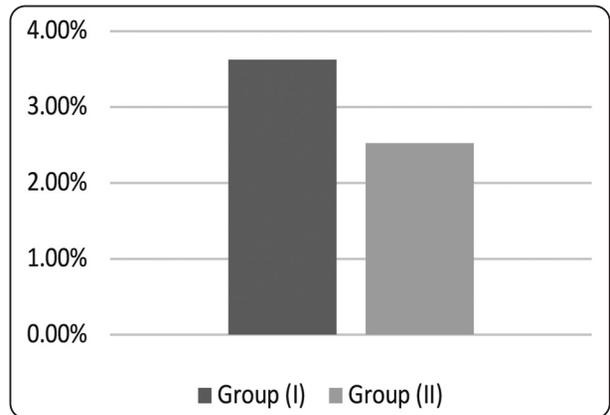


Fig (7): Bar chart showing average area percentage of new bone formation (%) for different groups

DISCUSSION

This clinical comparative study aimed to compare the histological and radiographical outcome of horizontal ridge augmentation after application of EDTA on the surface of cortical bone versus bone decortication. Despite the numerous studies describing the benefits of acids demineralization and bone decortications, there has been no studies describing the effect of EDTA gel on bone surface.

Adequate width and height of alveolar bone are mandatory for a successful placement of a dental implant at the recipient site. Absence of bone at the implant site, can be caused by either periodontitis, tooth extraction, or trauma due to long-term use of a removable prosthesis. In such case , a surgical

procedure, known as guided bone regeneration (GBR), can be used to restore bone height and width (*Lekovic et al., 1998; McAllister and Haghighat, 2007; Ong et al. 2008*).

In our study, mid-crestal incision was the incision of choice as it support blood perfusion to the edges of the flap with no risk of necrosis; making the incision in the area of the avascular zone which is located in the mid crest of the ridge prevents the risk of cutting through anastomoses (*Kleinheinz et al., 2005*). Two vertical releasing incisions were utilized to accommodate the increased dimension of the grafted ridge, allow for visibility of the edges of the membrane apically, ease of membrane manipulation during the bone fixation process and ease of periosteal incision to allow readaptation of soft tissue before tension free closure (*Urban, 2017*).

To improve bone grafts, decortication of the receptor bone bed have been recommended as proved by an experimental study on thirty six white rabbit. It was found that the bone density increased on sites of bone perforation and there was increased levels of VEGF, Type 1 collagen and Osteopontin (*Faria et al. 2008*). Other studies stated that the addition of bone inducers at the interface between grafts and receptor bone enhances bonding. The latter was first used by **Rezende et al., 2014** who stated the advantages of demineralization over the other methods.

In this study, comparison has been done between two different method of graft bed interface treatments. Graft integration into native bone will be enhanced by making bone penetrations into bone marrow to allow for blood to fill the graft space and increase cellular recruitment and this will lead to increasing the physical bond between the graft and the native bone (*Carvalho et al., 2000; Lundgren et al., 2000*).

Bone decortication was an integral step of GBR procedures. This was attributed to the increased source of undifferentiated mesenchymal cells that will increase blood supply and new bone formation

(*Buser et al., 1993*). *Alberius et al.* found that penetration of the bony cortex also increase the mechanical interlocking of the bone graft to recipient bed, which improves its stability (*Alberius et al., 1996*).

On the other hand, decortication, perforation have multiple limitations as increased bleeding and difficult visibility of the operative field (*Carvalho et al. 2000; Lundgren et al., 2000*).

Rezende et al., 2014, showed that using bone surface demineralization is better than mechanical bone decortication. Bone remodeling begins with dissolution of minerals by acids from osteoclasts that enzymatically digest the organic bone matrix (*Melcher, 1976*)

Demineralizing agents have been widely used to isolate collagen (*Pang et al., 2021*). This is why a method for bone demineralization using EDTA was chosen, bone tissue is formed by osteoinductive factors contained within the organic matrix. Demineralized fragments of bone induce bone formation subcutaneously and intramuscularly in rats. It was demonstrated that the demineralization process releases BMPs, which induce stromal cells to differentiate into osteoblasts (*Urist and McLean 1965; Urist et al., 1970; Urist, 1973*).

Although bone demineralization is successful in increasing the osteoinductive potential of bone grafts, in situ demineralization of the contacting surfaces between the bone graft and bone bed has never been used to improve the graft consolidation till Rezende et al. in 2014, studied the citric acid demineralizing effect on the graft bed interface (*Rezende et al., 2014*).

In previous studies the reaction rate, demineralization efficiency, and the effect on residual collagen were addressed. A comparison of 0.1 M EDTA and 0.6 M HCl for evaluating the efficiency of mineral removal and collagen integrity from bone revealed that EDTA resulted in an almost intact collagen structure, while the HCl destroyed the collagen structure. Thus, EDTA aids in removing min-

eral and preserving collagen integrity, but it takes longer treating time. (*Pang et al., 2021*).

EDTA Gel was proved to be a calcium chelating agent that results in removal of calcium ions from their hydroxy appetite crystals leading to exposure of the collagen fibers and other stimulatory proteins that promote osteoblastic differentiation and proliferation such as bone morphogenetic protein (*Gandolfi et al. 2019*)

The supersaturated concentration of EDTA gel was chosen in this study as it is the best concentration for chelation of calcium and the most efficient rate of demineralization with time (*Blomlöf et al. 1997*).

Certain inclusion criteria are required to select appropriate barrier membranes these include biocompatibility, and clinical controllability. Although collagen membranes show effective regeneration, yet their major limitation is their fast resorption, which results in early loss of barrier function. The pericardium membrane, the choice for this study, in comparison to collagen membranes have shown an effective crosslinking, suggesting its prolonged resorption time, it also has exceptional handling properties (*Muto et al. 2009; Gupta and Gupta 2014*).

Using deproteinized bovine bone mineral (DBBM) in this study was due to its slow rate of resorption, act as an osteoconductive scaffold to enhance bone regeneration outside the skeletal envelope and also it has no osteoinductive effect that can interfere with the osteoinductive effect of demineralization of the bone bed (*Hämmerle et al., 2008; Aludden et al., 2020; Lee, 2021*).

In this study, CBCT was chosen for the analysis of osseous changes. CBCT uses a two-dimensional detector to scan the head, rather than stacking multiple slices together, as the conventional CT scanner does. It also, does not expend high radiation doses in addition to providing a 3D information (*Sukovic, 2003*).

The timing for core biopsy was decided based on studies showed that the area % of new bone

significantly increased with the use of DBBM and resorbable barrier membrane after 6 months post-operatively (*Naenni et al., 2017; Lee, 2021*)

Every effort was taken in biopsy procedure to make sure that we evaluate the quality of newly formed bone. Trepine drill was used to obtain the biopsies which were immediately placed in a container filled with 10 % formalin for 5 days. Once fixed, then decalcified by immersing in 12% EDTA for 10 days then using ascending concentrations of alcohol (from 96 to absolute alcohol), each specimen was dehydrated, and then transferred to xylol to free it from alcohol then embedded into paraffin wax to be sliced to semi-thin sections of about 4 microns thick. Sections were transferred in descending concentrations of alcohol solutions (96%, 70%, and then distilled water). (*Bancroft, 2008*)

Masson trichrome stain was used for the histomorphometric analysis of bone quality and quantity as secondary outcome because it can differentiate between mineralized and osteoid tissue. (*Suvik, 2012*)

Histological evaluation of the core biopsies conducted 6 months after augmentation. In group I, histological analysis showed increased width of bone trabeculae and more osteoid tissue than Group II as well as basophilic immature collagen areas of woven bone or osteoid tissue which were indicative of the active new bone formation, The edges of the graft showed osteoclastic activity followed by bone matrix formation consistent with remodeling. Group I showed more obvious crosslinking between graft and bed, with shared marrow spaces and trabeculae of newly formed bone, impairing the identification of boundaries of graft, new bone, and recipient bed.

It was found that preosteoblast differentiate upon recognition of a rough surface and begin to deposit new bone. This explains the better results found in demineralized specimens in this study. Osteoblastic differentiation is stimulated by the release of BMPs by the demineralization process they in turn diffuse through the tissue (*Urist, 1973; Schwartz et al.*

2000). From a histomorphometric standpoint, the highest mean value of new bone was recorded in group I (EDTA group), with a highly statistically significant difference between the two groups.

Regarding CBCT results, both groups showed significant gain in width after six months. In comparison between the two groups, a non-significant difference in baseline measurements were recorded. However, after six months group I (EDTA group) showed higher mean increase in bone width (8.17 ± 0.99) in comparison to (6.37 ± 0.77) in group II (decortication group), with statistically significant difference between the two groups.

Based on the results of the present study we found that, demineralization by EDTA resulted in significantly more area % of newly formed bone and more bonding of this new bone to the graft and recipient bed compared to the decortication Group II. The bone width of EDTA Group I was significantly higher than those of the decortication group after 6 months according to the statistical analysis.

This study raises the possibility that demineralization of the contacting bone surfaces in the bone grafts and native bone can accelerate and intensify the mechanical interlocking of these grafts to the host bed.

CONCLUSION

Demineralization of alveolar bone is an effective way to increase the integration of bone graft and promote the new bone formation whenever ridge augmentation is needed as it has an osteoinductive effect on the osteoblastic cell differentiation and proliferation with no trauma to the alveolar ridge specially in very thin ridge. Decortication of alveolar bone is effective method to enhance blood supply and nourish the area with the undifferentiated mesenchymal cells which will aid in success of the augmentation procedures but in case of thin ridge the volume will be affected. Bone demineralization results in more width gain than mechanically decorticating the alveolar bone..

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